

Proceedings of the Annual International Conference of the IEEE Engineering in Medicine and Biology Society

Volume 14

PARIS, FRANCE

October 29 - November 1, 1992

Edited by

Jean Pierre Morucci

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AN EMG CONTROLLED PROSTHETIC FOREARM IN THREE DEGREES OF FREEDOM USING ULTRASONIC MOTORS

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ABSTRACT This paper discusses an EMG controlled prosthetic forearm with three degrees of freedom actuated by small size ultrasonic motors. Its weight is less than 700 g and the size is the same as the adult's arm. It produces no motion noise. In addition, it is possible to control six kinds of motions i.e. pronation and supination of the forearm, flexion and extension of the wrist, and grasping and hand-opening.

1. INTRODUCTION

An EMG controlled forearm with three degrees of freedom using small size ultrasonic motors was developed. The arm has six functions, i.e. hand-opening and grasping, wrist flexion and extension, and forearm pronation and supination. Also, we propose a limb function discrimination method where the electrode positions are made relatively free by utilizing the s-information among multi-channel EMG signals.

2. PROSTHETIC FOREARM USING ULTRASONIC MOTOR

Fig.1 shows a prosthetic forearm which was developed on an experimental basis. It is driven by ultrasonic motors installed in the forearm, wrist and hand, and has three degrees of freedom, i.e., six kinds of wrist flexion, wrist extension, forearm pronation, forearm supination, hand grasping and hand opening. Table 1 shows the specifications of the developed prosthetic forearm.

3. AMPUTEE-PROSTHESIS INTERFACE

Fig. 2 shows a block diagram of the amputee-prosthesis interface for controlling the arm. The surface EMG is measured from a part of the muscles which have actuated the original limb, and the motion intended by the amputee, such as flexion, extension, pronation, supination, grasping and hand-opening, is estimated. In parallel, the muscle force is estimated from the EMG signals. Then the electrical drive to control the prosthesis is produced from both.

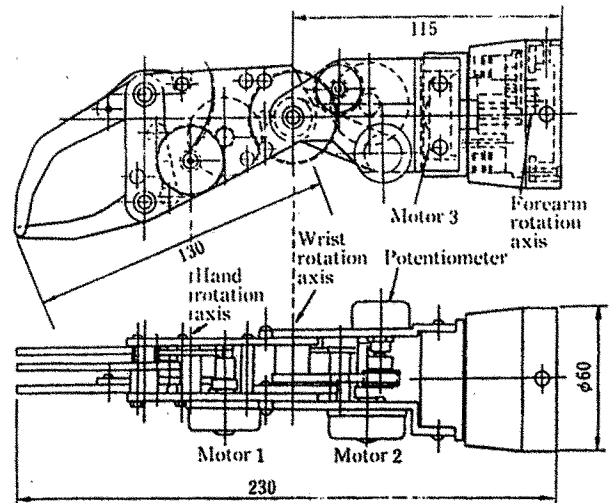


Fig.1 Prosthetic forearm with three degrees of freedom

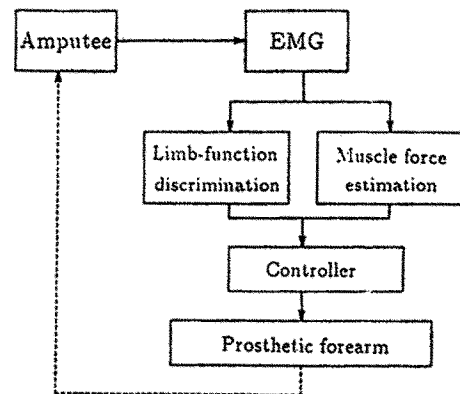


Fig.2 Amputee-prosthesis interface

Table 1 Specifications of the prosthetic forearm with three degrees of freedom

	Motions	Movable range (the time required)	Holding force	Gear ratio
Forearm	Pronation-supination	162° (0.6~30 s)	1.71 kg-cm	4.5
Wrist	Flexion-extension	135° (1.1~20 s)	10.40 kg-cm	17.5
Hand	Grasping-opening	105 mm (1.1~50 s)	4.16 kg	29.8

4. LIMB-FUNCTION DISCRIMINATION BY NEURAL NETWORK

Fig.3 shows a flow chart of the limb-function discrimination procedure proposed here, which is composed of band-pass filters, rectification, smoothing filters and neural network.¹⁾⁻⁵⁾

(1) Band-pass filter

The raw EMG signals measured at the surface of the amputee's skin are passed through the band-pass FIR filters. Then each of the four channel EMG signals is divided into three band frequency components.

(2) Rectification and Smoothing

The 4×3 EMG signals obtained from the band-pass filters are rectified and passed through individual one-pole Butterworth filters each with a low pass cutoff frequency of 1 Hz.

(3) Neural network

A feedforward type neural network is used to classify the rectified and smoothed EMG signals. The neural network consists of an input layer of 4×3 units, a hidden layer of ten units, and an output layer of 6 units. Each unit of the output layer represents one of six kinds of motions.

(4) Network pretraining

Four pairs of surface electrodes were attached on the forearm, 7 cm from the elbow joint. The electrode is dry-type made by Imasen Technical Lab. Three kinds of electrode arrangements are shown in table 1. EMG signal in each channel was A/D converted with the sampling frequency of 1 KHz and were stored in the computer as the data file.

After attaching the prosthetic forearm, the amputee is asked to perform each of six kinds of motions by one time. Then each of the stored EMG data was divided into 10 data sets of 200 msec intervals. The neural network is trained by error back propagation algorithm using these 6×10 data.

(5) Function discrimination

It is assumed that the amputee intends to make one of six motions. Since each unit of the output layer has the sigmoidal function, the output value is within 0 and 1. When one of the units of the output layer is more than 0.5 and all the others are less than 0.3, it is concluded that the motion assigned to the unit with the value more than 0.5 is intended by the amputee. Unless these conditions are satisfied, the discrimination is left undetermined.

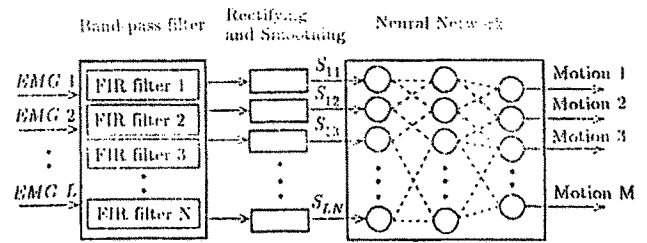


Fig.3 A limb function discrimination method using the neural network

5. DISCRIMINATION RATE AFTER LEARNING

Separately from training data, each of six kinds of motions were performed by 100 times and the EMG signals were used to confirm the function discrimination after learning.

Table 2 represents number of learning iterations, success rates and undetermined rates in different experiment conditions, where the success rate is the ratio of the correct discriminations in discriminated trials and the undetermined rate is the ratio of the undetermined trials in all trials. They are averages over ten kinds of initial values of the network weights. Note that the success rates are more than 90% independently of subjects and electrode locations, and especially the numbers of iterations training the neural networks are less than 30.

6. CONCLUSION

we developed an EMG controlled prosthetic forearm with three degree of freedom using small size ultrasonic motors. It was shown that the prosthetic forearm was well controllable by the amputee. Future research will be directed to develop a small size control box and more lightweight forearm which can be actually fitted.

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Table 2 Motion discrimination rates

Experiment	No. 1	No. 2	No. 3	No. 4	No. 5
Subject	Normal A	Normal A	Normal B	Normal B	Amputee
Electrode locations					
Number of iterations	20.1	17.8	9.0	26.0	14.9
Success rates (%)	100.0	100.0	92.7	95.5	93.5
Undetermined rates (%)	3.6	5.7	8.7	12.0	13.4

(Average values for 10 kinds of initial values of the synaptic weights)